

Simulating Self-Motion I: Cues for the Perception of Motion

L. R. Harris^{2,3,4}, M. R. Jenkin^{1,4}, D. Zikovitz^{3,4}, F. Redlick^{3,4}, P. Jaekl^{2,4}, U. T. Jasiobedzka^{1,4}, H. L. Jenkin^{2,4}, R. S. Allison^{1,4}

Centre for Vision Research, ¹Department of Computer Science, ²Department of Psychology and ³Department of Biology, York University; ⁴Centre for Research in Earth and Space Technology, Toronto, Ontario, Canada

Abstract: When people move there are many visual and non-visual cues that can inform them about their movement. Simulating self-motion in a virtual reality environment thus needs to take these non-visual cues into account in addition to the normal high-quality visual display. Here we examine the contribution of visual and non-visual cues to our perception of self-motion. The perceived distance of self-motion can be estimated from the visual flow field, physical forces or the act of moving. On its own, passive visual motion is a very effective cue to self-motion, and evokes a perception of self-motion that is related to the actual motion in a way that varies with acceleration. Passive physical motion turns out to be a particularly potent self-motion cue: not only does it evoke an exaggerated sensation of motion, but it also tends to dominate other cues.

Keywords: Proprioception; Self-motion; Visual and non-visual cues to motion

Introduction

A fundamental goal of virtual reality is to provide a user with a compelling sensation of an alternate environment. The process of simulating the changing visual view that observers would see if they were really moving around the simulated environment has tended to dominate virtual reality research, while other cues associated with self-motion are often ignored – though some haptic self-motion cue systems have been constructed (e.g. [1,2]), and auditory self-motion cues have been studied as well (see [3]). It is, however, a tribute to the flexibility of the human sensory system that providing only visual information in a virtual reality stimulation works as well as it does. Indeed, even just moving the user's view from one point to another without the user actually selecting where to go, or physically moving at all, can provide a compelling sense of self-motion.

There are two basic aspects to simulating motion in a virtual reality system. Firstly, how do viewers inform the virtual reality generator where they are and where they would like to move to in the environment? Secondly, how are viewers' movements within the environment actually simulated so as to provide them with a convincing and accurate sensation that they really have moved?

These problems are inter-related, since how viewers control the simulation contributes to their experience. If the user just sits in a chair and controls their motion around the virtual world with a joystick, then almost all of the cues to motion need to be simulated. At the other end of the spectrum, if viewers inform the generator about their movements by actually making complete and natural movements, then many of the natural non-visual cues to motion will be present, and there will be no need to simulate them. Even in this case,

differences between actual and simulated environments need to be taken into account. For example making people walk over real sand when simulating a desert scene might not be a practical solution.

In practice, the design of most virtual reality systems falls somewhere between these extremes, allowing the viewer to make some natural movements while simulating others. Typically, for example, virtual reality explorers are allowed and encouraged to move their heads, but not to leave a small working area.

In this paper we review the various sensory cues normally associated with self-motion. We then describe a series of experiments that quantify how much each cue contributes to the perception of self-motion, and assess how important it is to include each cue in a successful virtual reality simulation.

The Cues to Self-Motion

Vision

There are two classes of visual cues to self-motion: displacement and optic flow. Displacement refers to the fact that during movement, the locations of visual features are displaced relative to the viewer. When judging self-motion, particular features can be chosen, such as landmarks, and motion can be estimated in response to 'sightings' of these landmarks. However, navigation by sighting such features is clumsy as it requires regular checks and feedback. Using visual displacement does not easily allow anticipation of the results of a movement.

A second visual cue to motion results from the continuous movement of the images of all objects in the environment relative to the viewer, which creates a complex pattern of retinal motion referred to as optic flow [4,5]. Optic flow contains information about the amplitude and direction of the linear and rotational components of the self-motion that created the flow [6,7]. People can use optic flow, even when it is the only cue, to assess their direction of travel [8–11], though whether optic flow is used to guide navigation in humans is uncertain [6,12–15]. The magnitude of the translational component of self-motion is present in the flow field, but the mathematics of extracting it – especially in the presence of rotational components or object motion – is not trivial [16].

When optic flow occurs in the absence of other sensory cues to motion, it can evoke postural

adjustments [17,18] and the perception of actual self-motion, even though the viewer is stationary. This visually induced illusory sensation of motion is called *vection* and has associated perceptions of displacement and speed [19,20]. It has recently been shown that honey bees can use optic flow to judge flown distances [21–23]. Below we describe experiments that show that humans can also judge distance travelled from optic flow cues [24].

Gravito-inertial Force

Any movement of the body that changes its velocity induces forces on the body itself and on the organs and structures within it. This includes gravity but not constant velocity movement, which cannot generate any such forces. Within the body there are a number of sensory systems that can transduce the physical forces acting upon it. Some systems are specialised for doing so, such as the vestibular system and, less well known, a system based in the kidneys. Other systems are incidentally stimulated, for example the skin where it receives pressure from a support surface [25,26].

The vestibular system is a set of specialised gravito-inertial detecting organs located in the vestibule of the inner ear (see [27–29] for comprehensive reviews). The system is made up of the semicircular canals and the otoliths, which detect angular and linear accelerations of the head respectively [30]. Both parts are mechanical force transducers and are thus only sensitive to accelerations. Neither part is sensitive to the other type of acceleration: the otoliths are not sensitive to angular accelerations and the semicircular canals are not sensitive to linear accelerations.

Accelerations on the body are also sensed internally by specialised visceral graviceptors, especially in the region of the kidney [31]. It is unlikely that these organs provide a very quantitative directional estimate of linear accelerations and, of course, they are subject to the same confusion between gravity and self-motion as other accelerometers. Their properties have been investigated by centrifuging patients with spinal lesions at various levels with their otoliths close to the axis of rotation, and thus not subject to centrifugal forces [31].

The somatosensory (touch) system includes a number of mechano-receptors that detect pressure and stretch on the skin and in muscles, joints and visceral organs when the body is accelerated [25]. Seated subjects undergoing acceleration have the cutaneous receptors in the back, bottom and feet stimulated by the forces generated by the acceleration. Although there is evidence from patients with spinal

lesions that the somatosensory system does not contribute significantly to our perception of self-motion [32], the lack of such sensation when undergoing accelerations may detract from the veracity of the simulation.

Detecting air flow over the skin is a special case of somatosensory perception. Although at normal walking velocities the flow of air over the skin is probably too slow to provide useful cues to motion, at faster speeds, especially those taking place without a windshield (such as when simulating cycling, skiing or the flight of a hang glider), there is a strong expectancy of air flow over the skin, which may also provide quantitative perceptual cues about the motion. Airflow is important to birds, which will start flying when airspeed reaches a certain magnitude [33,34] and can enhance their visual reflexes to movement [35].

Since all of the above gravito-inertial, force-sensitive systems are normally activated together, it is really of only academic interest which sub-system makes which contribution to the overall perception [36]. People can use physical motion alone to assess a position change [37–43] or their direction of travel [44,45].

The gravito-inertial-somatosensory system as a whole, comprising all of the components described above, has three drawbacks when applied to the tasks of detecting and measuring self-motion in an environment:

- It detects forces and therefore only acceleration from which position has to be derived.
- It cannot distinguish gravity from any other accelerations, and thus always provides a 'vector sum' of gravity with any other applied forces.
- The vestibular system reports only on the movement of the head, and thus motion about the body itself must be derived from the partially known relationship between the head and body.

The fact that the otoliths only sense acceleration can theoretically be turned to advantage when simulating motion in virtual reality and in more traditional flight simulators. As long as the appropriate onset cue accelerations are presented to the operator, periods of constant velocity can be ignored as far as stimulating physical cues go as they are invisible to the vestibular system. The position of limited-range equipment can be reset during such movements using accelerations below threshold (around 0.1 m/s² [46], although reported values range from 0.014 to 0.25 m/s² [29]). This procedure is known as 'washout'.

The fact that gravity is indistinguishable from other accelerations can also potentially be turned to advantage by tilting observers and encouraging them to

believe that the component of acceleration of gravity now in the horizontal plane of the head is actually due to a linear movement [47].

Proprioception

Proprioception refers to knowledge of the body in general. As such, many of the systems considered above qualify as proprioceptors – even some aspects of visual processing. Here we refer specifically to that part of the proprioceptive system comprising the mechano receptors of the joints and muscles from which the position of the individual joints and therefore limbs can be reconstructed [48]. Proprioception can provide powerful information about self-motion [49]. For example, knowing about the movement of the feet during walking and the length of the stride carries enough information to calculate the distance covered.

There is a very variable linkage between limb movement and distance travelled so proprioceptive information concerning movement can only be interpreted in context. The relationship is very different between running and walking, for example, and almost non-existent when using a vehicle. Even when riding a bicycle, gears change the relationship between limb and body movements. Clearly, if proprioception is to be useful, a very flexible calibration between limb movement and distance is needed. We describe below some experiments showing that, after training, limb movement can be used with some degree of precision.

Efferent Copy

In 1950, Holst and Mittelstaedt ([50], and see [31] for an updated review) demonstrated that actively moving insects have access to a simultaneous copy of their efferent motor commands. This pioneering work led to an extensive search for evidence of an efference copy in all animals. Cells have recently been found in the parietal cortex of monkeys that change their sensory fields before an intended gaze shift [51]. Also, cells receiving vestibular information seem to be able to distinguish between self-generated and externally applied movements [52,53] implying the existence of an efference copy modifying the sensory information during the movement.

Having access to a copy of the efferent command allows the brain to prepare for the consequences of an intended motion before it has occurred. A mismatch between expected (efferent) and actual (sensory) movement is a likely cause of motion sickness [54], and probably also contributes to cybersickness [55].

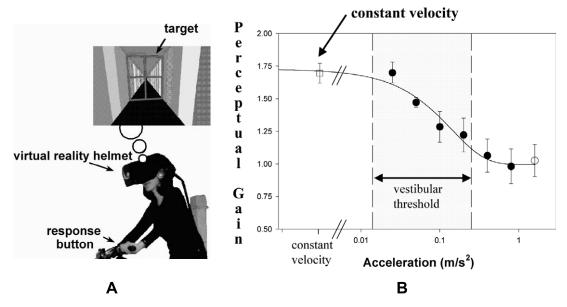


Fig. 1. (a) Experimental set up. Subjects sat passively on a bicycle (cf. Fig. 5). Target distances were presented in a virtual environment as a frame in a corridor. When the subject had a good estimate of the distance, obtained using perspective and parallax cues, the target disappeared and visual movement down the corridor commenced. Subjects indicated when they had gone through the target distance. (b) The data are expressed as the ratio between the perceived movement (the target distance) to the actual motion (the optic flow) which we refer to as the perceptual gain, plotted as a function of the simluated acceleration down the corridor. Redrawn from [21].

Like proprioception, an efference copy has a very variable linkage with the resulting movement, and needs to be interpreted in context. The copy of the motor command to move the hands when turning the steering wheel of a car has to be matched with sensory information that is far removed from the musculature of the arms in order to inform the brain that the car has gone round a corner successfully, according to plan.

Efference copy is a central but often neglected component in the design of virtual reality systems. The control system that has been chosen, for example driving a vehicle, pedalling a bike or pushing a joystick, needs a motor output from the observer, and a copy of this output will then be matched with the sensory result. The expected sensory result of a self-motion is a multisensory barrage that includes components from all the systems mentioned above. Calibrating the connection between the motor signal out and the sensory signal that comes back often requires extensive learning by the subject.

How Much Does Each of the Cues Contribute to Self-Motion Perception?

Here we summarise a set of experiments we have conducted to assess the contribution of optic flow activating the visual system, gravito-inertial cues activating the gravito-inertial-somatosensory system, limb movements activating the proprioceptive system, and the knowledge of the intention to move. In these experiments we measure our perception of self-motion by measuring how far a subject perceives themselves to have moved in response to controlled presentation of various cues. Critical to these experiments has been the development of a device to present visual and non-visual cues within a virtual reality environment over extended physical distances. This was accomplished through the design and use of a virtual reality system based on a tricycle 'Trike', the details of which are described in a companion paper [56].

Measuring how far someone perceives they have moved presents some interesting methodological considerations. Simply asking people to estimate how far they have moved requires them to make a relative judgement against an internalised yardstick. Distortions in the representation of the yardstick, such as stimulus compression or expansion [38,57] when judging multiples of the yardstick, complicate the interpretation of such data. Such a technique cannot be used to measure the accuracy with which people perceive their movement through a particular distance. Asking subjects to reproduce previously travelled distances [40] also does not address the veridicality of perception, since an inaccuracy or systematic bias in the

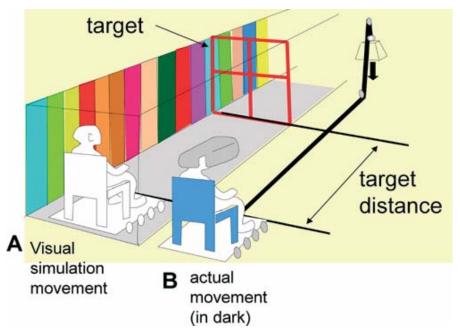


Fig. 2. The experimental setup used to investigate the perception of physical motion. Targets were presented in a virtual corridor. When the subject had obtained an estimate of its distance they started the trial. The screen went dark and subjects were pulled along by means of a falling weight attached to their chair by a rope and pulley. Accelerations of between 0.1 and 0.5 m/s² for about 3 m could be obtained. Visual targets were presented either in a real corridor (see insert to Fig. 3) or via an HMD (above).

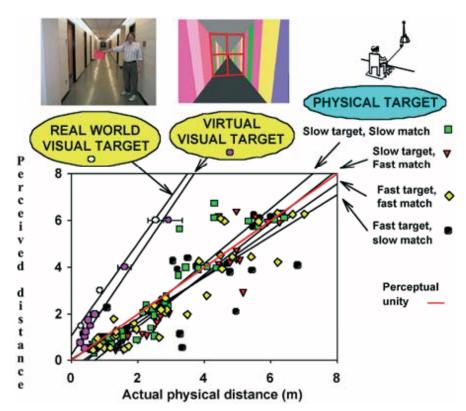


Fig. 3. The perceptual response to physical motion. When presented with a target distance by being physically moved through it (physical target), subjects were able to reproduce the target distance accurately (light square, triangle, diamond and filled square symbols, reflecting various combinations of accelerations of the target and test motions). When target distances were presented visually either in the real world (hollow circles: real target) or in the head mounted display (filled circles: virtual target) subjects consistently and dramatically overestimated their movement and indicated that they had passed through the target distance after only travelling about $\frac{1}{3}$ of that amount. Redrawn from [40].

perception of the initial distance may be matched by similar inaccuracy and bias in the measurement trials.

For all the experiments described below, the following technique was used. Subjects were presented with a given target distance that they were asked to remember. Visual targets were presented within the virtual reality display as a large frame within a corridor. This is illustrated in Figs 1a and 2, and in the inserts to Fig 3. Subjects were encouraged to obtain parallax cues as to the distance of this target, as well as using perspective cues. The target was then removed and various cues to self-motion were presented in each experiment. Subjects indicated when they had travelled through the previously indicated distance.

Measuring the Effectiveness of Visual Cues to Motion

To measure how well subjects judge distance travelled with only visual cues, we first presented them with the visual target in a virtual corridor to generate an internal representation of a distance (Fig. 1 [24]). The target was then removed and the subjects were then presented with optic flow commensurate with travelling down the corridor. They were then asked to indicate when they had moved through the remembered target distance. In addition to presenting optic flow consistent with constant velocity movement down the corridor, we also used a smooth, linear movement with a constant acceleration to generate data that could be compared to gravito-inertial-somatosensory data (see below), where accelerations are required for the system to work at all.

Interestingly, how far subjects thought they had moved depended upon the movement profile. We describe the response as a 'perceptual gain' (vertical axis of Fig. 1b), in which the distance they perceived themselves to have moved (i.e. the target distance they were originally given) is expressed as a fraction of the distance they actually moved (the cumulative effect of optic flow they considered equivalent to this distance). A high perceptual gain thus corresponds to subjects perceiving that they have gone further than the actual motion, and a low perceptual gain corresponds to less sensation of motion.

There are two main features depicted in the data shown in Fig. 1. Firstly, lower accelerations ($<0.1 \text{ m/s}^2$) and constant velocity (0.4-6.4 m/s) motion profiles are associated with higher perceptual gains than higher accelerations ($>0.1 \text{ m/s}^2$). This is illustrated by the shape of the curve in Fig. 1 which forms a sigmoid between the higher and lower gains as a function of

acceleration. Secondly, lower accelerations ($<0.1 \text{ m/s}^2$) are associated with perceptual gains greater than unity, whereas higher accelerations are associated with accurate judgements, i.e. a perceptual gain close to unity. The former effect indicates a variation of the effectiveness of visual optic flow cues as a function of acceleration of self-motion; the latter indicates a miscalibration between actual and perceived motion.

The variation in perceptual gain with acceleration cannot be explained as a general distortion of space within the virtual reality display. The target distances were the same for all motion profiles, and yet led to very different perceptual judgements. The effects must be due to the optic flow itself. All the constant velocity trials were associated with similar perceptual gains, which were statistically independent of velocity over the range tested (0.4-6.4 m/s). While it remains possible that motion noise, such as jerkiness introduced by pixelation, might affect perceived motion [58-60], the consistency across all speeds shown in our constant velocity data suggests that our results for low acceleration movement are unlikely to be explained by such inadequacies of the display. The results are consistent with a variation in the processing of optic flow that depends upon the self-motion profile. Constant acceleration conditions were chosen to cover the range from the lowest accelerations that were practical with our experimental setup, to accelerations above the reported threshold for the vestibular system. Constant velocity conditions where chosen over the range practical with the experimental setup, and included velocities associated with normal walking and cycling.

Subjects were deprived not only of non-optic-flow visual cues to their motion, but also of vestibular, somatosensory and proprioceptive cues that would normally provide complementary information. For example, the otolith division of the vestibular system, the inner-ear organs stimulated by physical linear acceleration, normally plays a major role in humans' perception of self-motion, providing the movement has accelerations above vestibular threshold [40,61,62]. For whole-body linear acceleration, the vestibular threshold seems to be around 0.1 m/s² (although studies have reported values ranging from $0.014-0.25~\text{m/s}^2$ [27,46]). This acceleration range corresponds to the range of optic flow accelerations associated with the transition between high and low perceptual gains (Fig. 1b).

Higher perceptual gains are associated with optic flow accelerations that would normally not be accompanied by other cues, especially vestibular cues. The higher gains suggest that more emphasis is placed on visual information when other information is scarce, and that the visual contribution is toned down or given

lower weighting when other information is also available (as it is for other aspects of perception, e.g. [63]). The only problem with this apparently logical argument is that optic flow seems to be too effective at evoking a sensation of self-motion. Visual perceptual gains are often too large, with constant velocity motion being associated with a perception of moving 1.7 times faster than the stimulus motion. Reducing the perceptual gain to unity hardly represents giving vision a lower weighting that allows other senses to contribute. Why might this be?

Our visual display was quite impoverished. The spatial resolution was quite poor with pixels subtending about 0.3° and the field was of a limited extent. There were no binocular or stereoscopic cues to the structure of the world, and accommodation was fixed optically. However, it seems counterintuitive that a paucity of visual cues might be enhancing our subjects' sensation of self-motion.

The structure of our display was a simple 2 m-wide corridor with no texture on the floor or ceiling. These dimensions mean that subjects were less than 1 m (orthogonally) from each of the walls. It is well known anecdotally that riding in a low-slung vehicle or travelling along a narrow tunnel can enhance the sensation of speed of motion. The high perceptual gains experienced by our subjects might be related to this observation.

Measuring the Effectiveness of Gravito-inertial-somatosensory Cues

To measure the role of gravito-inertial-somatosensory cues used alone, subjects sat on a chair mounted on a wheeled platform that could be moved at a constant acceleration (Fig. 2). They were first given a target distance (either the same one as used in the vision experiments or a real target presented in a real corridor or by being physically moved in the dark through the target distance). They were then moved in complete darkness and indicated when they perceived they had traversed the target distance.

For constantly accelerating movement of between 0.1 and 0.3 m/s² and for visual targets presented either via a HMD or as a real target, the perceptual gain was about three (Fig. 3). That is, when the chair had moved one metre, it was perceived as moving three times further. Over this same range of accelerations, the perceptual gain of the response to optic flow was between 1.0 and 1.2 (see Fig. 1). That is, the perceived distance of physical motion in the dark was perceptu-

ally equivalent to about three to four times the visual motion. For physically presented targets, subjects were quite successful in reporting the correct distance, even when a deliberate mismatch was introduced between the motion profile used for target presentation and test runs (see Fig. 3).

Israël et al. [39] matched a visually presented target distance with physical motion over very short distances, and also found that subjects needed less physical motion (0.24 m) to match a visual distance (0.8 m). This over-estimation, by a factor of between three and five for acceleration values around 0.5 m/s², was also found when subjects were asked to estimate displacement in metres [64], for motion along the z-axis through the top of the head [65] and under active motion conditions [41].

Interactions between Visual and Vestibular Contributions

By moving people on the chair mounted on a wheeled platform while they were wearing a virtual reality helmet (Fig. 2), we were able to control visual and nonvisual sensory inputs independently. The perceived distance of self-motion when visual and physical cues indicated different distances at the same time were more closely perceptually equivalent to the physical motion experienced, rather than the visual stimulation. Thus, when a range of visual movements was paired with a single physical motion, subjects estimated them to be almost the same. There was a small contribution from the visual information that could be modelled as [66,67]:

Perceived distance=(k_{vis} * visual d)+(k_{vest} * physical d) where:

$$\begin{split} &k_{vis}\text{=}weighting of visual signal=0.14} \\ &k_{vest}\text{=}weighting of vestibular signal=0.83} \\ &visual d\text{=}distance signalled by optic flow} \\ &physical d\text{=}distance subject physically moved} \end{split}$$

Measuring the Effectiveness of Proprioceptive Cues

To assess the significance of the proprioceptive input to the perception of moved distance, we repeated our experiments wearing a HMD on a stationary exercise bicycle mounted on rollers. Since the bicycle did not move, there were no gravito-inertial cues to motion. We presented the targets as before, and asked subjects to cycle to their remembered locations in the dark. Because of the arbitrary coupling between the pedals

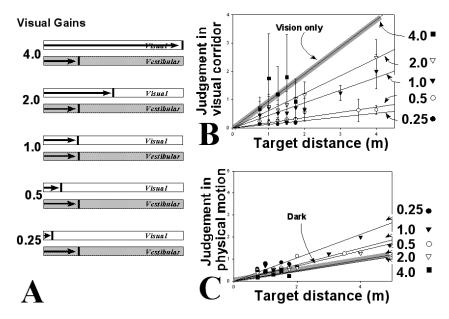


Fig. 4. Physical motion and visual cues were presented at the same time but with different distances of motion (a). Thus there were two 'right' answers when indicating the distance traversed, derived either from the optic flow or the physical cues to motion. Graph (b) shows the perceived distance (horizontal axis) as a function of the actual visual distance traversed (vertical axis) for different accelerations (m/s^2) . The same data are replotted in graph (c) as a function of the physical distance. Data cluster when plotted against the physical distance indicating that physical cues were more important than visual motion in determining the perception of motion. Redrawn from [62].

and the road wheels, we first trained our subjects to pedal at constant acceleration, and thus calibrated the pedalling action to an expected movement down a corridor.

The experiments described above looking at visual and physical sensory cues did not show range effects. That is, the perceptual gain appeared to be constant over the full range of distances tested. The effect of pedalling, however, did depend upon the distance of the targets to which the subject was pedalling. For closer targets, subjects tended to overshoot (Fig. 5) and pedal past the target. This behaviour corresponds to a perceptual gain of less than one. However for targets around 15 m, performance became accurate (perceptual gain 1), and for further targets, subjects actually stopped short of the target, indicating a perceptual gain greater than one. This was especially true for lower accelerations (0.05 m/s²). For these low accelerations, the visual perceptual gain would be high (Fig. 1), and the vestibular contribution close to threshold.

Intention to Move (Efference Copy)

The pedalling experiments cannot isolate the role of efference copy – the neural equivalent of expectation –

from the other cues. The proprioception from pedalling is always matched to the efference copy of the motion commands, since the pedalling was performed actively by the subjects. To explore these more sophisticated aspects of the cues to self-motion, we have developed TRIKE. TRIKE is an instrumented tricycle that can be ridden in the real world, while the subject is immersed in a virtual world. By dissociating the direction that the subject moves in the virtual world from his or her movements in the real world, we hope to look at the contribution of efference copy. This is the subject of ongoing research.

Discussion

Using an experimental technique of matching the perceived distance of motion to various cues and their combinations, we have assessed the significance of each cue to the perception self-motion. Optic flow cues evoked an accurate sensation for high accelerations, but created the perception of moving too far at low accelerations, especially at constant velocity. Since virtual reality often tries to simulate motion of the operator entirely by visual cues, this perceptual overestimation is highly significant, especially under conditions when it is important to judge movements

PEDALLING ONLY

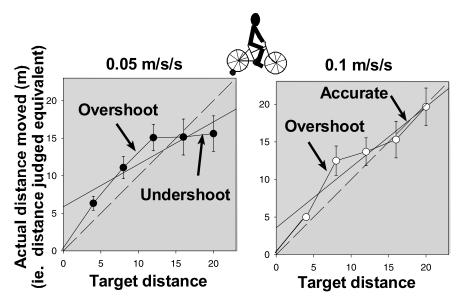


Fig. 5. Proprioceptive and efference copy cues to motion. The distance cycled on a stationary exercise bike in the dark (vertical axis) judged as corresponding to a perceived distance (horizontal axis). For target distances below 15 m subjects tended to pedal slightly too far indicating a perceptual gain of less than one. However the predominant feature is accurate performance with perceptual gain reaching a minimum of 0.8. Two cycling accelerations are shown, 0.05 m/s^2 (left) and 0.1 m/s^2 (right).

accurately. Examples include aircraft taxiing simulations, driving simulators, and using virtual reality to control remote vehicles or robots. In contrast, this overestimation may be highly desirable to create a more exciting ride in entertainment applications.

Surprisingly, physical motion is also over-estimated, and by an even greater amount, with perceptual gains around three for accelerations above 0.1 m/s². Thus, adding physical motion cues would not be expected to reduce the over-estimation of visually induced movement. Indeed, when both visual and physical forces were passively presented simultaneously, the non-visual cues dominated, suggesting various strategies for virtual reality designers to control the perceived distance of motion in virtual reality through manipulation of the physical motion of the operator.

The cues associated with active movement do seem to act as a brake on the high perceptual gains associated with the passive reception of visual and physical forces. When subjects actively pedalled to targets, especially close targets, they were relatively accurate, and if anything overshot the targets, implying an underestimate of how far they had pedalled. So by using active movements in a virtual environment, the high perceptual gains associated with passive movement might be avoided.

This may be related to the anecdotal phenomenon of distances seeming longer the first time they are travelled in a car. For the outward journey no efference copy or expectancy can exist, and the traveller needs to rely on predominantly visual optic flow cues. These have been found to lead to over-estimation of distances, especially at the near-constant velocity of a car. Coming back, after an expectancy has been set up, the distance is no longer over-estimated.

Are the accurate perceptions of active movements due to proprioceptive cues from the limbs or to using a copy of the motor commands? TRIKE has been developed partly to answer these questions by allowing us to decouple the link between limb movement and intended movement.

If it is important to use active movements, what movements contribute, perceptually, as 'active'? Clearly, natural movements like walking and running are active, but what of the minor motor movements of the feet and hands used for the active control of vehicles such as cars? Consider the act of pushing a joystick forward to control forward motion. How does this contribute to the perception of self-motion? Experiments are underway to compare passive and actively controlled movements using both full physical movement by pedalling the TRIKE, or by more subtle manipulations of the expected and actual movements.

Acknowledgements

We would like to acknowledge our indebtedness to Jim Zacher and Jeff Laurence whose technical contributions made the experiments described here possible. The research was funded by the Natural Science and Engineering Research Council of Canada (NSERC) and the Centre for Research in Earth and Space Technologies (CRESTech) of Ontario.

References

- Iwata H, Yano H, Nakaizumi F. (2001) Gait master: a versatile locomotion interface for uneven virtual terrain. In: Proc IEEE Virtual Reality 131–137
- Barbagli F, Ferrazzin D, Avizzano AC, Bergamasco M. (2001) Washout filter design for a motorcycle simulator. In: Proc IEEE Virtual Reality 225–232
- 3. Kayahara T, Sato T. (2001) Auditory motion induced by visual motion and its dependence on stimulus size. In: Proc IEEE Virtual Reality 241–245
- 4. Gibson JJ. (1950) The perception of the visual world. Boston: Houton Mifflin
- Cutting JE. (1986) Perception with an eye for motion. Cambridge, MA: MIT Press
- Harris LR. (1994) Visual motion caused by movements of the eye, head and body. In: Smith AT, Snowden RJ (Eds). Visual Detection of Motion. London: Academic Press
- Lappe M, Bradley RJ, Harris RA. (2000) Neuronal processing of optic flow. San Diego, CA: Academic Press
- Royden CS, Banks MS, Crowell JA. (1992) The perception of heading during eye-movements. Nature 360: 583– 587
- 9. Warren WH, Morris MW, Kalish M. (1988) Perception of translation heading from optical flow. J Exp Psychol Hum Percep and Perf 14: 646–660
- Warren WH, Blackwell AW, Kurtz KJ, Hatsopoulos NG, Kalish ML. (1991) On the sufficiency of the velocity field for perception of heading. Biol Cybern 65: 311–320
- 11. Lappe M, Rauschecker JP. (1994) Heading detection from optic flow. Nature 369: 712–713
- Harris LR. (1997) The coding of self motion. In: Harris LR, Jenkin M (Eds). Computational and psychophysical mechanisms of visual coding. Cambridge: Cambridge University Press
- Lappe M, Bremmer F, van den Berg AV. (1999) Perception of self motion from visual flow. Trends in Cog Sci 3: 329–336
- Harris JM, Rogers BJ. (1999) Going against the flow. Trends in Cog Sci 3: 449–450
- Wann J, Land M. (2000) Steering with or without the flow: is the retrieval of heading necessary? Trends in Cog Sci 4: 319–324
- Longuet-Higgins HC, Prazdny K. (1980) The interpretation of a moving retinal image. Proc Roy Soc Lond B: Biol Sci 208: 385–397
- Redfern MS, Furman JM. (1994) Postural sway of patients with vestibular disorders during optic flow. J Vestib Res 4: 221–230
- van Asten WN, Gielen CCAM, Denier van der Gon JJ. (1988) Postural adjustments induced by simulated motion of differently structured environments. Exp Brain Res 73: 371–383
- Previc FH. (1992) The effects of dynamic visual stimulation on perception and motor control. J Vestib Res 2: 285–295

- Howard IP, Howard A. (1994) Vection: the contributions of absolute and relative visual motion. Percept 23: 745– 751.
- Srinivasan MV, Zhang SW, Lehrer M, Collett TS. (1996) Honey-bee navigation en route to the goal: visual flight control and odometry. J Exp Biol 199: 237–244
- Srinivasan MV, Zang S, Bidwell N. (1997) Visually mediated odometry in honeybees. J Exp Biol 200: 2513– 2522
- 23. Srinivasan MV, Zhang S, Altwein M, Tautz J. (2000) Honeybee navigation: nature and calibration of the 'odometer'. Science 287: 851–853
- Redlick FP, Harris LR, Jenkin M. (2001) Humans can use optic flow to estimate distance of travel. Vis Res 41: 213–219
- 25. Lackner JR. (1992) Multimodal and motor influences on orientation: implications for adapting to weightless and virtual environments. J Vestib Res 2: 307–322
- Mergner T, Rosemeier T. (1998) Interaction of vestibular, somatosensory and visual signals for postural control and motion perception under terrestrial and microgravity conditions – a conceptual-model. Brain Res Rev 28: 118– 125.
- Benson JA. (1980) Burst reset and frequency control of the neuronal oscillators in the cardiac ganglion of the crab, Portunus-Sanguinolentus. J Exp Biol 87: 285–313
- Wilson VJ, Melvill Jones G. (1979) Mammalian vestibular physiology. Plenum: New York
- Howard IP. (1982) Human visual orientation. New York: Wiley
- Lowenstein OE. (1974) Comparative morphology and physiology. In: Kornhuber HH (Ed). Handbook of sensory physiology. The vestibular system. New York: Springer-Verlag
- 31. Mittelstaedt H. (1997) Interaction of eye-, head-, and trunk-bound information in spatial perception and control. J Vestib Res 7: 283–302
- 32. Walsh EG. (1961) Role of the vestibular apparatus in the perception of motion on a parallel swing. J Physiol (Lond.) 155: 506–513
- 33. Bilo D. (1983) A neck flexion related activity of flight control muscles in the flow-stimulated pigeon. J Comp Physiol 153: 111–122
- 34. Bilo D. (1992) Optocollic reflexes and neck flexionrelated activity of flight control muscles in the airflowstimulated pigeon. In: Berthoz A, Graf W, Vidal PP (Eds). The head-neck sensory motor system. Oxford: Oxford University Press
- 35. Gioanni H, Sansonetti A. (1999) Characteristics of slow and fast phases of the optocollic reflex (OCR) in head free pigeons (Columba livia): influence of flight behaviour. Eur J Neurosci 11: 155–166
- 36. Seidman SH, Paige GD. (1998) Perception of translational motion in the absence of non-otolith cues. Soc Neurosci Abstr 24: 162.10
- Mayne R. (1974) A systems concept of the vestibular organs. In: Kornhuber HH (Ed). Handbook of sensory physiology. vestibular system. New York: Springer-Verlag
- Parker DE, Wood DL, Gulledge WL, Goodrich RL. (1979) Self-motion magnitude estimation during linear oscillation: changes with head orientation and following fatigue. Aviation, Space and Environmental Medicine 50: 1112– 1121
- Israël I, Chapuis N, Glasauer S, Charade O, Berthoz A. (1993) Estimation of passive horizontal linear-wholebody displacement in humans. J Neurophysiol 70: 1270– 1273
- 40. Berthoz A, Israël I, Georges-Francois P, Grasso R, Tsuzuku T. (1995) Spatial memory of body linear displacement: what is being stored? Science 269: 95–98

- Loomis JM, Klatzky RL, Golledge RG, Cicinelli JG, Pellegrino JW, Fry PA. (1993) Nonvisual navigation by blind and sighted: assessment of path integration ability. J Exp Psychol (Gen) 122: 73–91
- Glasauer S, Amorim MA, Vitte E, Berthoz A. (1994) Goaldirected linear locomotion in normal and labyrinthinedefective subjects. Exp Brain Res 98: 323–335
- Harris LR, Jenkin M, Zikovitz DC. (2000) Visual and nonvisual cues in the perception of linear self motion. Exp Brain Res 135: 12–21
- 44. Ohmi M. (1996) Egocentric perception through interaction among many sensory systems. Cog Brain Res 5: 87–96
- Telford L, Howard IP, Ohmi M. (1995) Heading judgements during active and passive self-motion. Exp Brain Res 104: 502–510
- Gundry AJ. (1978) Thresholds of perception for periodic linear motion. Aviat Space Environ Med 49: 679–686
- Parker DE, Reschke MF, Arrott AP, Lichtenberg BK, Homick JL. (1985) Otolith tilt-translation reinterpretation following prolonged weightlessness – implications for preflight training. Aviat Space Environ Med 56: 601–606
- Matthews PBC. (1988) Proprioceptors and their contribution to somatosensory mapping – complex messages require complex processing. Can J Physiol and Pharm 66: 430–438
- Hlavacka F, Mergner T, Bolha B. (1996) Human selfmotion perception during translatory vestibular and proprioceptive stimulation. Neurosci Lett 210: 83–86
- Holst EV, Mittelstaedt H. (1950) Das Reafferenzprinzip. Naturwissenschaften 37: 464–476
- Duhamel JR, Colby CL, Goldberg ME. (1992) The updating of the representation of visual space in parietal cortex by intended eye-movements. Science 255: 90–92
- Gdowski GT, Boyle R, Mccrea RA. (2000) Sensory processing in the vestibular nuclei during active head movements. Archives Italiennes de Biologie 138: 15–28
- 53. Roy JE, Cullen KE. (2001) Selective processing of vestibular reafference during self-generated head motion. J Neurosci 21: 2131–2142
- 54. Oman CM. (1998) Sensory conflict theory and space sickness: our changing perspective. J Vestib Res 8: 51–56
- Lo WT, So RH. (2001) Cybersickness in the presence of scene rotational movements along different axes. Appl Ergon 32: 1–14

- Allison R, Harris LR, Hogue A, Jasiobedzka U, Jenkin H, Jenkin M, Jaekl P, Laurence J, Pentile G, Redlick F, Zacher J, Zikovitz D. (2002) Simulating self motion II: a virtual reality tricycle. Virtual Reality 6(2): 86–95
- 57. Stevens SS. (1955) The measurement of loudness. J Acoust Soc Am 27: 815–829
- 58. Treue S, Snowden RJ, Andersen RA. (1993) The effect of transiency on perceived velocity of visual patterns: a case of 'temporal capture'. Vis Res 33: 791–798
- 59. Troscianko T, Fahle M. (1988) Why do isoluminant stimuli appear slower? J Opt Soc Am A 5: 871–880
- Zanker JM, Braddick OJ. (1999) How does noise influence the estimation of speed? Vis Res 39: 2411–2420
- Benson AJ, Spencer MB, Scott JR. (1986) Thresholds for the detection of the direction of whole-body, linear movements in the horizontal plane. Aviat Space Environ Med 57: 1088–1096
- 62. Israël I, Berthoz A. (1989) Contribution of the otoliths to the calculation of linear displacement. J Neurophysiol 62: 247–263
- Landy MS, Maloney LT, Johnston EB, Young M. (1995) Measurement and modeling of depth cue combination: in defense of weak fusion. Vis Res 35: 389–412
- 64. Golding JF, Benson AJ. (1993) Perceptual scaling of whole-body low frequency linear oscillatory motion. Aviat Space Environ Med 64: 636–640
- Young LR, Markmiller M. (1996) Estimating linear translation: saccular versus utricular influences. J Vestib Res 6: \$13
- Harris LR, Jenkin M, Zikovitz DC. (1999) Vestibular cues and virtual environments: choosing the magnitude of the vestibular cue. In: IEEE Int Conf on Virtual Reality 1: 229–236
- Jenkin M, Harris LR, Redlick F, Zikovitz D. (1999) The same perception of self motion from different combinations of visual and non-visual cues. Percept 28 (Suppl): 2c

Correspondence and offprint requests to: M. R. Jenkin, Centre for Vision Research and Department of Computer Science, York University, 4700 Keele St, Ontario, M3J 1P3 Canada. Email: jenkin@cs.yorku.ca